



# Electrostatic charge on spacer devices and salbutamol response in young children

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## Abstract

Electrostatic charge on plastic spacer devices may affect the efficacy of inhaled drugs, but its consequences have never been evaluated in asthmatic children with airflow limitation. At the end of a positive metacholine challenge, 64 children ( $51.3 \pm 12.9$  months, 32 boys, specific airway resistance (SRaw)  $257.1 \pm 56.7\%$  and forced expiratory volume in 1 s (FEV<sub>1</sub>)  $64.2 \pm 17.9\%$  of the predicted value) inhaled one puff of hydrofluoroalkane-134a (HFA-134a) salbutamol (Ventoline®), and 15 min later two other puffs (total dose of 300 µg), delivered through either a new static Babyhaler® ( $n = 21$ ), a detergent-coated, reduced static, Babyhaler® ( $n = 20$ ), or a metal NES-Spacer® ( $n = 23$ ) equipped with facemask. SRaw and FEV<sub>1</sub> were measured after each treatment and compared between groups by a Kruskal–Wallis test. The first 100 µg salbutamol induced a  $151.7 \pm 43.9\%$  decrease in SRaw and a  $19.9 \pm 10.6\%$  increase in FEV<sub>1</sub>. Additional 200 µg salbutamol allowed a supplementary decrease of  $35.1 \pm 25.7\%$  in SRaw and increase of  $12.1 \pm 11.8\%$  in FEV<sub>1</sub>, without significant difference between the spacer devices. Electrostatic charge on spacer devices does not affect bronchodilation with HFA-134a salbutamol in metacholine-challenged pre-school children. This could be in part explained by the use of supramaximal doses of salbutamol.

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## 1. Introduction

Pressurised metered-dose inhalers (pMDIs) attached to spacer devices are widely used for delivering anti-asthma medications and, in pre-school children, are even considered as the best method of inhaled treatments delivery (O'Callaghan, 1997; Warner and Naspitz, 1998). However, drug delivery from spacer devices may be affected by various factors, such as spacer volume, type of valve, dead space between inlet

and outlet valve, electrostatic charge, spacer emptying pattern, mode of inhalation breathing, and the drug–spacer combination (Bisgaard, 1999; Dolovich, 1999; O'Callaghan and Barry, 2000; Dubus et al., 2001).

Electrostatic charge is inherent to the non-conducting surface of plastic spacer devices. The higher the electrostatic charge is, the higher is the amount of aerosolised drug attracted to the wall of the plastic spacer device, and, thus, retained within the spacer device (O'Callaghan et al., 1993). In vitro studies, all demonstrate that the drug output from an electrostatically charged spacer device is considerably decreased when compared with an electrostatically reduced or a metal non-electrostatic spacer device

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(Bisgaard, 1995; Dewsbury et al., 1996; Wildhaber et al., 1996a,b; Barry and O'Callaghan, 1997; Berg et al., 1998). Moreover, electrostatic charge increases the variability of dose delivery (Janssens et al., 1999; Wildhaber et al., 2000a,b). Scintigraphic studies with labelled salbutamol and budesonide show that the reduction in the electrostatic charge of the plastic spacer devices induces a 10–35% increase in lung deposition in children and adults with asthma (Kenyon et al., 1998; Piérart et al., 1999; Wildhaber et al., 2000a,b). Two pharmacokinetic studies demonstrate that the electrostatic charge in plastic spacers decreases the delivery of salbutamol to the lungs with an approximate twofold reduction in lung bioavailability either with Volumatic® (Glaxo-SmithKline, Paris, France) in adults (Clark and Lipworth, 1996) and Babyhaler® (Glaxo-SmithKline) in children (Anhoj et al., 1999). A recent pharmacodynamic study, conducted in 20 volunteers adults with a bronchodilator responsive airflow limitation, shows that a 10% increase in pulmonary function is obtained with less salbutamol when using treated rather than untreated Volumatic® (Wildhaber et al., 2000a,b). Conversely, in a crossover study conducted in 90 young children with stable asthma, the change in peak expiratory flows measured after inhalation of HFA-salbutamol from the non-static NES-Spacer® (AstraZeneca, Nanterre, France) compared with static plastic spacer devices or the same plastic spacer devices treated to eliminate static charge are the same (Dompeling et al., 2001). Therefore, such results might be different in asthmatic children with bronchial obstruction.

This study was undertaken to assess whether the use of small volume spacer devices with different electrostatic charge affected the bronchodilator response of cumulative doses of hydrofluoroalkane-134a (HFA-134a) salbutamol on the recovery from metacholine-induced bronchoconstriction in pre-school children with asthma.

## 2. Material and methods

### 2.1. Patients

Children between ages 3 and 6 years with a clinical diagnosis of asthma (Warner and Naspitz, 1998) and a positive metacholine challenge were recruited from

December 1999 to December 2000. These children had been sent to the Laboratory by their paediatrician or pulmonologist to perform pulmonary function tests (PFTs) with a metacholine challenge. Over 1 year, 87 children were tested. Among them, 2 were unable to perform PFTs, 21 had a negative metacholine challenge, and 64 met the inclusion criteria. When satisfying the criteria, children were asked to participate to the bronchodilator challenge. Data on asthma were obtained by delivering a questionnaire to the parents. This study was approved by the local ethics committee and informed written consent was obtained from all the families.

### 2.2. Metacholine challenge

All baseline PFTs were performed between 09:30 and 12:00 h. Parents were instructed to withhold any kind of anti-asthmatic, anti-histamine or inhaled therapy for 24 h before the tests. Children with a concomitant upper airway infection or asthma exacerbation, which could have influenced the PFTs, were excluded. The PFTs consisted of a flow volume spirometric test and SRaw measurements with a constant body plethysmograph (model Master Lab Jaeger, Wurzburg, Germany), using a method that we have previously described in such young children (Badier et al., 1999). The mean of five reproducible measurements was used each time. To improve reproducibility, we used a computer game where children had to blow four candles on the screen of the computer. The functional measurements were compared with the predictive values of Zapletal (Zapletal et al., 1987).

Metacholine challenge was performed only if a normal baseline test was obtained, i.e. a value of specific airway resistance (SRaw)  $\leq 120\%$  of the predicted value and a value of forced expiratory volume in 1 s (FEV<sub>1</sub>)  $\geq 80\%$  of the predicted value. For metacholine inhalation, a standardised dosimeter technique was used. Metacholine puffs were delivered by a dosimeter (MEFAR dosimeter, Electromedicalli, Brescia, Italy): air driving pressure = 1.65 kg/cm<sup>2</sup>; air flow rate = 70–75 l/min; particle size = 0.5–4  $\mu\text{m}$ . Two parameters were adjusted before the test: a nebulisation time of 1.2 s and a pause time of 5 s between two puffs. A metacholine solution of 2 mg/ml was used and 3 ml of the solution was placed in the nebuliser (20  $\mu\text{g}$  of metacholine delivered per puff). Cumulative doses of

metacholine (40, 60, 100, 100  $\mu\text{g}$  and a further 100  $\mu\text{g}$  if necessary in order to reach the maximal dose of 400  $\mu\text{g}$ ) were administered. SRaw and FEV<sub>1</sub> measurements were performed 2 or 3 min after each inhaled dose of metacholine. Because of the well known difficult reproducibility of spirometric measurements in the pre-school children, the metacholine challenge was considered positive when a twofold increase of SRaw was obtained. The concentration of metacholine which produced this twofold increase of SRaw, or provocative dose, was noted.

### 2.3. Salbutamol challenge

When the metacholine challenge was positive, we administered one puff, followed 15 min later by two individual puffs, of HFA-134a salbutamol pMDI (Ventoline<sup>®</sup>, Glaxo-SmithKline; one puff = 120  $\mu\text{g}$  salbutamol sulphate = 100  $\mu\text{g}$  salbutamol base) through one of the following spacer devices equipped with its own facemask: a brand new electrostatically charged 350 ml Babyhaler<sup>®</sup> which had been stored in its original plastic bag, an electrostatically reduced 350 ml Babyhaler<sup>®</sup>, and a metal non-electrostatic 250 ml NES-Spacer<sup>®</sup> (also called Nebuchamber<sup>®</sup>). The method used to reduce the electrostatic charge on Babyhaler<sup>®</sup> consisted of soaking the spacer for a few minutes in a detergent solution (Palmolive<sup>®</sup>, 1:5000 dilution) and to allow it to drip-dry for 12–24 h before use (Piérart et al., 1999). Each spacer device was new before use. Spacer devices were used in a random order. The salbutamol pMDI was vigorously shaken and primed by firing two puffs in the room. The child was instructed to breath quietly into the spacer device via the face mask. Then, one puff was delivered into the spacer device and inhaled in five quiet respiratory cycles allowing the valves to move. SRaw and FEV<sub>1</sub> measurements were performed 15 min after the inhalation. Then, two other individual puffs of Ventoline<sup>®</sup> were administered in the same conditions than previously described and followed by a last PFT 15 min later. Pulsed oxymetry and heart beat were recorded during all the procedure.

### 2.4. Statistical analysis

The results were expressed as means ( $\pm$ S.D.) and compared between the three groups by a

Kruskal–Wallis non-parametric ANOVA. The bronchodilator response was measured as a difference between pre-treatment and post-treatment values of SRaw and FEV<sub>1</sub>, and was expressed in percent of the predicted value (Waalkens et al., 1993; Chrystyn, 1994).  $\Delta_{100\mu\text{g}}\text{SRaw}$  and  $\Delta_{100\mu\text{g}}\text{FEV}_1$  represented the difference between the post-metacholine value of the respective spirometric indices and the value obtained after the inhalation of 100  $\mu\text{g}$  salbutamol.  $\Delta_{200\mu\text{g}}\text{SRaw}$  and  $\Delta_{200\mu\text{g}}\text{FEV}_1$  represented the difference between the post-100  $\mu\text{g}$  salbutamol value of the respective spirometric indices and the value obtained after the inhalation of 200  $\mu\text{g}$  salbutamol.  $\Delta_{300\mu\text{g}}\text{SRaw}$  and  $\Delta_{300\mu\text{g}}\text{FEV}_1$  represented the difference between the post-metacholine value of the respective spirometric indices and the value obtained after the inhalation of the total dose of salbutamol, i.e. 300  $\mu\text{g}$ . A *P* value <0.05 was considered significant.

## 3. Results

No metacholine-challenged child refused to participate to the study and all children achieved successfully the bronchodilator protocol. Tolerance was excellent and no side effect was noted. The main characteristics of the 64 children are presented in Table 1. Their mean age was  $51.3 \pm 12.9$  months. There was 32 boys (50%). The mean standing height was  $103.0 \pm 8.4$  cm and the mean weight was  $16.8 \pm 3.9$  kg, without significant difference between the three groups. The children were in majority (59.4%), treated with long-term inhaled steroids administered through a spacer device. No long-term bronchodilator treatment was prescribed. The values of baseline PFTs were in the normal range for all children. The provocative dose of metacholine for doubling SRaw was higher in the NES-Spacer<sup>®</sup> group than in the two others but without significant statistical difference. The level of metacholine-induced bronchoconstriction was similar in the different groups.

Results of the salbutamol challenge are reported in Table 2 concerning the SRaw values and in Table 3 concerning FEV<sub>1</sub> values. No difference was noted at any dose of salbutamol between the three groups for the spirometric values. One puff of Ventoline<sup>®</sup> (100  $\mu\text{g}$  salbutamol) allowed a mean  $151.7 \pm 43.9\%$  decrease in SRaw and a mean  $19.9 \pm 10.6\%$  increase in FEV<sub>1</sub>.

Table 1  
Characteristics of the asthmatic children with results expressed as mean  $\pm$  S.D.

	Children inhaling from a brand new Babyhaler® ( <i>n</i> = 21)	Children inhaling from a detergent-coated Babyhaler® ( <i>n</i> = 20)	Children inhaling from a metallic NES-Spacer® ( <i>n</i> = 23)
Age (months)	51.4 (13.9)	51.6 (11.6)	50.9 (13.7)
Proportion of boys	<i>n</i> = 12 (57.1%)	<i>n</i> = 10 (50%)	<i>n</i> = 10 (43.5%)
Positive prick-tests	<i>n</i> = 10 (47.6%)	<i>n</i> = 10 (25.0%)	<i>n</i> = 8 (34.8%)
Inhaled corticosteroids	<i>n</i> = 13 (61.9%)	<i>n</i> = 11 (55.0%)	<i>n</i> = 14 (60.9%)
Baseline SRaw <sup>a</sup> (% predicted)	80.7 $\pm$ 22.1	85.5 $\pm$ 21.8	79.4 $\pm$ 17.8
Baseline FEV <sub>1</sub> <sup>b</sup> (% predicted)	105.6 $\pm$ 10.9	101.3 $\pm$ 15.7	104.9 $\pm$ 13.5
Provocative dose ( $\mu$ g)	206.7 $\pm$ 117.2	207.1 $\pm$ 120.2	256.9 $\pm$ 102.8

<sup>a</sup> SRaw: specific airway resistance.

<sup>b</sup> FEV<sub>1</sub>: forced expiratory volume in 1 s.

Table 2  
Improvement in SRaw<sup>a</sup> in asthmatic children receiving one puff and then two puffs of HFA-134a salbutamol (total dose of 300  $\mu$ g) via three different electrostatically charged spacer devices (results are expressed as mean  $\pm$  S.D. and compared by a Kruskal–Wallis test)

	Children inhaling from a brand new Babyhaler® ( <i>n</i> = 21)	Children inhaling from a detergent-coated Babyhaler® ( <i>n</i> = 20)	Children inhaling from a metallic NES-Spacer® ( <i>n</i> = 23)	<i>P</i> value
SRaw values (% predicted)				
Post-metacholine SRaw	262.8 $\pm$ 58.9	264.5 $\pm$ 64.3	244.0 $\pm$ 46.9	0.59
Post-100 $\mu$ g salbutamol SRaw	115.1 $\pm$ 40.4	106.6 $\pm$ 28.3	94.4 $\pm$ 29.7	0.09
Post-300 $\mu$ g salbutamol SRaw	76.2 $\pm$ 22.2	66.1 $\pm$ 14.4	66.3 $\pm$ 13.9	0.17
Differences (% predicted)				
$\Delta_{100 \mu\text{g}} \text{SRaw}^{\text{b}}$	-148.0 $\pm$ 43.3	-157.9 $\pm$ 50.0	-149.6 $\pm$ 40.0	0.80
$\Delta_{200 \mu\text{g}} \text{SRaw}^{\text{c}}$	-37.9 $\pm$ 29.4	-40.5 $\pm$ 20.2	-28.1 $\pm$ 26.0	0.16
$\Delta_{300 \mu\text{g}} \text{SRaw}^{\text{d}}$	-186.6 $\pm$ 53.9	-198.4 $\pm$ 56.4	-177.7 $\pm$ 39.0	0.54

<sup>a</sup> SRaw: specific airway resistance.

<sup>b</sup>  $\Delta_{100 \mu\text{g}} \text{SRaw}$ : difference between post-100  $\mu$ g salbutamol SRaw and post-metacholine SRaw.

<sup>c</sup>  $\Delta_{200 \mu\text{g}} \text{SRaw}$ : difference between post-300  $\mu$ g salbutamol SRaw and post-100  $\mu$ g salbutamol SRaw.

<sup>d</sup>  $\Delta_{300 \mu\text{g}} \text{SRaw}$ : difference between post-300  $\mu$ g salbutamol SRaw and post-metacholine SRaw.

Table 3  
Improvement in FEV<sub>1</sub><sup>a</sup> in asthmatic children receiving one puff and then two puffs of HFA-134a salbutamol (total dose of 300  $\mu$ g) via three different electrostatically charged spacer devices (results are expressed as mean  $\pm$  S.D. and compared by a Kruskal–Wallis test)

	Children inhaling from a brand new Babyhaler® ( <i>n</i> = 21)	Children inhaling from a detergent-coated Babyhaler® ( <i>n</i> = 20)	Children inhaling from a metallic NES-Spacer® ( <i>n</i> = 23)	<i>P</i> value
FEV <sub>1</sub> values (% predicted)				
Post-metacholine FEV <sub>1</sub>	63.3 $\pm$ 20.5	61.5 $\pm$ 13.2	68.0 $\pm$ 20.1	0.47
Post-100 $\mu$ g salbutamol FEV <sub>1</sub>	83.1 $\pm$ 18.2	84.3 $\pm$ 16.9	86.2 $\pm$ 17.8	0.78
Post-300 $\mu$ g salbutamol FEV <sub>1</sub>	94.4 $\pm$ 13.9	95.0 $\pm$ 14.5	99.7 $\pm$ 11.2	0.43
Differences (% predicted)				
$\Delta_{100 \mu\text{g}} \text{FEV}_1^{\text{b}}$	18.9 $\pm$ 12.0	22.8 $\pm$ 9.8	18.2 $\pm$ 9.9	0.31
$\Delta_{200 \mu\text{g}} \text{FEV}_1^{\text{c}}$	12.0 $\pm$ 11.2	10.7 $\pm$ 14.1	13.4 $\pm$ 10.8	0.47
$\Delta_{300 \mu\text{g}} \text{FEV}_1^{\text{d}}$	31.1 $\pm$ 15.8	33.5 $\pm$ 10.5	31.7 $\pm$ 13.4	0.83

<sup>a</sup> FEV<sub>1</sub>: forced expiratory volume in 1 s.

<sup>b</sup>  $\Delta_{100 \mu\text{g}} \text{FEV}_1$ : difference between post-100  $\mu$ g salbutamol FEV<sub>1</sub> and post-metacholine FEV<sub>1</sub>.

<sup>c</sup>  $\Delta_{200 \mu\text{g}} \text{FEV}_1$ : difference between post-300  $\mu$ g salbutamol FEV<sub>1</sub> and post-100  $\mu$ g salbutamol FEV<sub>1</sub>.

<sup>d</sup>  $\Delta_{300 \mu\text{g}} \text{FEV}_1$ : difference between post-300  $\mu$ g salbutamol FEV<sub>1</sub> and post-metacholine FEV<sub>1</sub>.

The inhalation of two other puffs induced a supplementary decrease of  $35.1 \pm 25.7\%$  in SRaw and a supplementary increase of  $12.1 \pm 11.8\%$  in FEV<sub>1</sub>. At the end of the bronchodilator challenge, all children recovered SRaw values less than 120% and/or FEV<sub>1</sub> values greater than 80% of the predicted values. Fifty-five children (85.9%) had spirometric values higher than their baseline values at the end of the study.

#### 4. Discussion

In this pharmacodynamic study, we show in a group of 64 children, aged 3–6 years, with moderate provoked bronchial obstruction assessed either by SRaw or FEV<sub>1</sub> measurements, that there is no difference in bronchodilator response between a static plastic, a reduced static plastic and a metal spacer device.

Various techniques have been described to reduce the electrostatic charge on plastic spacers: by wiping the plastic spacer device with an anti-static cloth, by coating the inner walls with an anti-static lining, by priming the spacer device by firing placebo or drug doses so that the inner surfaces are coated with surfactant, or by washing the spacer device with water or a detergent solution (O'Callaghan et al., 1993; Clark and Lipworth, 1996; Dewsbury et al., 1996; Wildhaber et al., 1996a,b, 2000a,b; Barry and O'Callaghan, 1997; Berg et al., 1998; Kenyon et al., 1998; Piérart et al., 1999; Janssens et al., 1999). Using the same protocol that we used, Piérart (Piérart et al., 1999) found that the electrostatic charge was negligible on the surface of all detergent-coated spacer devices (less than  $1.2 \mu\text{C}/\text{m}^2$ , with C = Coulomb), regardless of the brand of detergent or the dilution used, and high on all non-coated spacer devices (greater than  $5 \mu\text{C}/\text{m}^2$ ). The mean lung deposition of five individual puffs (500  $\mu\text{g}$ ) of labelled chlorofluorocarbon (CFC) salbutamol in healthy adults was 11.5% when using a static spacer device compared to 45.6% when using a detergent-coated spacer device ( $P < 0.001$ ). In another study, the variability of the amount of salbutamol deposited in untreated spacer devices was also higher when compared to non-static spacer devices, with a coefficient of variation of 21% versus 13% (Wildhaber et al., 2000a).

We found that the pharmacodynamic effect of 100  $\mu\text{g}$ , and then of a total of 300  $\mu\text{g}$ , HFA-134a salbutamol was similar between the groups whatever

the electrostatic charge on spacer devices. We studied HFA-134a salbutamol in spite of everything because HFA is going to replace CFC in all pMDIs and because only HFA-134a Ventoline<sup>®</sup> is currently used in our country. Salbutamol was delivered from the Babyhaler<sup>®</sup>, but also from the NES-Spacer<sup>®</sup>, despite the fact that pMDI did not fit well in the metal spacer device, because in our experience a lot of patients use this combination of drug and spacer device.

Our results are in accordance with those obtained in children with stable asthma, where the mean difference of the change in peak expiratory flow between small non-electrostatic (NES-Spacer<sup>®</sup>) and large (Volumatic<sup>®</sup>) or small (Aerochamber<sup>®</sup>, Boehringer Ingelheim, Alkmaar, the Netherlands) electrostatic spacer devices was only +1.7% (–1.3 to 4.7%) after 100  $\mu\text{g}$  HFA-134a salbutamol and +1.9% (–1.4 to 5.1%) after 400  $\mu\text{g}$  HFA-134a salbutamol (Dompeling et al., 2001). However, a recent pharmacokinetic study conducted in five healthy children demonstrated that the inhalation of four single puffs of HFA-134a salbutamol (400  $\mu\text{g}$ ) through a new Babyhaler<sup>®</sup> or a new Aerochamber<sup>®</sup> induced a twofold decrease in both peak and average plasma salbutamol levels compared to the inhalation through a Babyhaler<sup>®</sup> coated with benzalkonium chloride (Anhoj et al., 1999).

Failure to identify significant in vivo differences between spacer devices with different electrostatic charge may have at least two causes. The first one is that we used supramaximal doses of salbutamol and that children who were challenged by metacholine were near their plateau with 100  $\mu\text{g}$  HFA-134a salbutamol, even delivered from a statically charged Babyhaler<sup>®</sup>. Consequently, differences found in in vitro, scintigraphic, and pharmacokinetic studies may be clinically irrelevant because of the optimal bronchodilation obtained with only 100  $\mu\text{g}$  salbutamol. The two pharmacodynamic studies conducted in children with asthma, i.e. that of Dompeling (Dompeling et al., 2001) and ours, support this hypothesis. The time course of bronchodilation may have also contribute to our apparent dose–response effect and be the explanation for the further bronchodilation seen after the second and third puff. The second possible cause is that the proposed benefits of anti-static devices are nullified by the inherent variability of salbutamol delivery from spacer devices due to breathing patterns of the children, handling of spacer devices, etc.

(Dewsbury et al., 1996; Janssens et al., 1999) and/or by the important amount of salbutamol available for inhalation because of the specific aerodynamic behaviour of HFA aerosol with spacer devices (Barry and O'Callaghan, 1997; Dubus et al., 2001). However, metacholine challenge does not mimic an acute asthma attack and our results might be different in "natural" and more severe bronchoconstriction.

In conclusion, this study demonstrates that the inhalation of HFA-134a salbutamol through differently electrostatically charged small volume spacer devices equipped with face masks induces a similar bronchodilation in asthmatic pre-school children with a metacholine-induced bronchoconstriction. Our findings only concern HFA-134a salbutamol, small volume spacer devices, and metacholine-challenged pre-school children.

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## References

- Anhoj, J., Bisgaard, H., Lipworth, B.J., 1999. Effect of electrostatic charge in plastic spacers on the lung delivery of HFA-salbutamol in children. *Br. J. Clin. Pharmacol.* 47, 333–336.
- Badier, M., Guillot, C., Dubus, J.C., 1999. Bronchial challenge with carbachol in 3–6-year-old children: body plethysmography assessments. *Pediatr. Pulmonol.* 27, 117–123.
- Barry, P.W., O'Callaghan, C., 1997. In vitro comparison of the amount of salbutamol available for inhalation from different formulations used with different spacer devices. *Eur. Respir. J.* 10, 1345–1348.
- Berg, E., Madsen, J., Bisgaard, H., 1998. In vitro performance of three combinations of spacers and pressurized metered dose inhalers for treatment in children. *Eur. Respir. J.* 12, 472–476.
- Bisgaard, H., 1995. A metal aerosol holding chamber devised for young children with asthma. *Eur. Respir. J.* 8, 856–860.
- Bisgaard, H., 1999. Future options for aerosol delivery to children. *Allergy* 54, 97–103.
- Chrystyn, H., 1994. Standards for bioequivalence of inhaled products. *Clin. Pharmacokinet.* 26, 1–6.
- Clark, D.J., Lipworth, B.J., 1996. Effect of multiple actuations, delayed inhalation and antistatic treatment on the lung bioavailability of salbutamol via a spacer device. *Thorax* 51, 981–984.
- Dewsbury, H.J., Kenyon, C.J., Newman, S.P., 1996. The effects of handling techniques on electrostatic charge on spacer devices: a correlation with in vitro particle size analysis. *Int. J. Pharm.* 137, 261–264.
- Dolovich, M., 1999. Aerosol delivery to children: what to use, how to choose. *Pediatr. Pulmonol.* 18, 79–82.
- Dompeling, E., Oudesluys-Murphy, A.M., Janssens, H.M., Hop, W., Brinkman, J.G., Sukhai, R.N., de Jongste, J.C., 2001. Randomised controlled study of clinical efficacy of spacer therapy in asthma with regard to electrostatic charge. *Arch. Dis. Child.* 84, 178–182.
- Dubus, J.C., Rhem, R., Dolovich, M., 2001. Delivery of HFA and CFC salbutamol from spacer devices used in infancy. *Int. J. Pharm.* 222, 101–108.
- Janssens, H.M., Devadason, S.G., Hop, W.C.J., Le Souëf, P.N., De Jongste, J.C., Tiddens, H.A.W.M., 1999. Variability of aerosol delivery via spacer devices in young asthmatic children in daily life. *Eur. Respir. J.* 13, 787–791.
- Kenyon, C.J., Thorsson, L., Borgström, L., Newman, S.P., 1998. The effects of static charge in spacer devices on glucocorticosteroid aerosol deposition in asthmatic patients. *Eur. Respir. J.* 11, 606–610.
- O'Callaghan, C., 1997. Delivery systems: the science. *Pediatr. Pulmonol.* 15, 51–54.
- O'Callaghan, C., Barry, P.W., 2000. How to choose delivery devices for asthma. *Arch. Dis. Child.* 82, 185–187.
- O'Callaghan, C., Lynch, J., Cant, M., Robertson, C., 1993. Improvement in sodium cromoglycate delivery from a spacer device by using an antistatic lining, immediate inhalation, and avoiding multiple actuations of drug. *Thorax* 48, 603–606.
- Piérart, F., Wildhaber, J.H., Vrancken, I., Devadason, S.G., Le Souëf, P.N., 1999. Washing plastic spacers in household detergent reduces electrostatic charge and greatly improves delivery. *Eur. Respir. J.* 13, 673–678.
- Waalkens, H.J., Merkus, P.J.F.M., van Essen-Zandvliet, E.E.M., Brand, P.L.P., Gerritsen, J., Duiverman, E.J., Kerrebijn, K.F., Knol, K., Quanjer, Ph.H., 1993. Assessment of bronchodilator response in children with asthma. *Eur. Respir. J.* 6, 645–651.
- Warner, J.O., Naspitz, C.K., 1998. Third international pediatric consensus statement on the management of childhood asthma. *Pediatr. Pulmonol.* 25, 1–17.
- Wildhaber, J.H., Devadason, S.G., Eber, E., Hayden, M.J., Everard, M.L., Summers, Q.A., Le Souëf, P.N., 1996a. Effect of electrostatic charge, flow, delay and multiple actuations on the in vitro delivery of salbutamol from different small volume spacers for infants. *Thorax* 51, 985–988.
- Wildhaber, J.H., Devadason, S.G., Hayden, M.J., James, R., Dufty, A.P., Fox, R.A., Summers, Q.A., Le Souëf, P.N., 1996b. Electrostatic charge on a plastic spacer device influences the delivery of salbutamol. *Eur. Respir. J.* 9, 1943–1946.
- Wildhaber, J.H., Waterer, G.W., Hall, G.L., Summers, Q.A., 2000a. Reducing electrostatic charge on spacer devices and bronchodilator response. *Br. J. Clin. Pharmacol.* 50, 277–280.
- Wildhaber, J.H., Janssens, H.M., Piérart, F., Dore, N.D., Devadason, S.G., Le Souëf, P.N., 2000b. High-percentage lung delivery in children from detergent-treated spacers. *Pediatr. Pulmonol.* 29, 389–393.
- Zapletal, A., Samanek, M., Paul, T., 1987. Lung function in children and adolescents: methods, reference values. In: Herzog, H. (Ed.), *Progress in Respiration Research*, Karger, Basel. pp. 114–218.